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(54) **Rapidly exchangeable coronary catheter.**

(57) A rapidly exchangeable balloon dilatation catheter for accessing the coronary arteries of a human comprising: an elongate wire-like shaft having proximal and distal ends and including a proximal tubular member formed from hypotubing (28). The shaft has sufficient column strength to enable it to be advanced through a patient's vasculature to the coronary arteries and the proximal tubular member has a lumen (36) extending through it.

A distal tubular member (32) is secured to the distal region of the shaft and is sufficiently flexible to access the coronary arteries but itself has insufficient column strength for such access without additional support. The distal tubular member (32) has an inflation lumen (40) extending longitudinally therein and a proximal end in fluid communication with the lumen (36) of the hypotubing, the inflation lumen (40) being in communication with a balloon inflation port (42). The distal tubular member (32) also includes a longitudinally extending guidewire lumen (44) to receive a guidewire (12) and distal and proximal ports (33,46), the guidewire lumen (44) extending from the distal region of the shaft to the distal end of the catheter and over a distance such that when a guidewire (12) is positioned through the guidewire lumen (44), the column strength of the distal tubular member (32) is increased, the

guidewire and the shaft together supplying support along the length of the catheter. An inflatable, relatively inelastic balloon (34) is mounted on the distal tubular member (32) with its distal end (54) sealingly attached to the distal end of the distal tubular member (32) and its interior in fluid communication with the inflation lumen (40) through the inflation port (42).

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This invention relates to balloon dilatation catheters and particularly to such catheters as are used in percutaneous transluminal coronary angioplasty.

Dilatation catheters, and particularly, those used for percutaneous transluminal coronary angioplasty (PTCA), typically include an elongate flexible shaft of the order of 150 cm long having a dilatation balloon mounted to the distal end of the shaft and an inflation lumen extending longitudinally within the shaft from its proximal end to the interior of the balloon so that the balloon may be inflated and deflated. Typically, such PTCA catheters also are provided with a full length guidewire lumen that is open at the distal tip of the shaft at a distal outlet opening. The proximal end of the guidewire lumen is open at the proximal end of the catheter. The guidewire lumen receives a guidewire which, when the guidewire and catheter are placed within a patient's artery, can be manipulated to guide the wire and catheter to the desired branch of the patient's arteries.

Typically, the balloon dilatation catheter and guidewire are guided to the entrance to the coronary arteries by a previously placed guide catheter. The guide catheter commonly is percutaneously inserted into the patient's femoral artery and is advanced along the aorta toward the heart. The guide catheter typically is provided with a preshaped distal tip adapted to remain at the coronary ostium leading to the coronary artery. Once placed, the guide catheter provides direct, quick access to the entrance to the coronary arteries.

It is common during a PTCA procedure for the physician to exchange the balloon catheter for another catheter, for example, if it is desired to change balloon sizes. This may occur, for example, if the physician initially performed a partial dilatation with a small diameter balloon and then wished to further dilate the patient's artery by using a catheter having a larger balloon. Such a catheter exchange may be accomplished in several ways. In one technique, the conventional guidewire which may be approximately 175 cm long is removed from the in situ balloon catheter and is replaced with a longer exchange wire, typically about 300 cm long. The length of the exchange wire that extends out of the patient is greater than the length of the balloon catheter thus providing a means by which the guidewire may be grasped at all times to prevent inadvertent withdrawal of the guidewire as the catheter is withdrawn. Once the catheter is withdrawn over the exchange wire, the next catheter can be threaded over the exchange wire and inserted into the patient, the exchange wire providing a direct path to guide the catheter to the portion of the artery to be dilated. If desired, the exchange wire then may be removed and replaced with a shorter conventional wire, although some

physicians may prefer to permit the exchange wire to remain in place for the remainder of the procedure.

Another technique omits the necessity for an exchange wire by providing a guidewire extension that is attached to the proximal end of the guidewire thereby effectively extending the length of the guidewire that protrudes out of a patient sufficiently to permit the catheter to be withdrawn and a new catheter to be threaded back into the patient without losing guidewire position.

Still another technique for performing a catheter exchange is that described in "New Instruments for Catheterization and Angiocardiology" by Bjorn Nordenstrom, *Radiology*, Vol. 85, 1965, pp. 256-259, which describes a catheter having a relatively short guidewire lumen at the distal end of the catheter, the guidewire lumen having a proximal terminal opening located distally of the proximal end of the catheter shaft. In this arrangement, the guidewire passes through the catheter shaft only for a segment of the length of the shaft. The catheter can be moved along the guidewire in the fashion of a "monorail". Because the guidewire lumen is relatively short and is considerably shorter than the overall length of the catheter, the catheter can be withdrawn from the patient over the original guidewire without dragging the guidewire out of the artery together with the catheter because the length of the guidewire protruding from the patient is longer than the length of the guidewire lumen of the catheter. Thus, a portion of the guidewire is exposed at all times and may be grasped by the physician.

Although the use of the monorail system facilitates catheter exchanges, the PTCA catheters in which the monorail system have been incorporated have presented some difficulties. One of the problems presented is that because the guidewire only extends through a relatively small portion of the overall length of the catheter, the remaining portion of the catheter shaft is unsupported by the guidewire. When the balloon catheter and guidewire are advanced through the guide catheter by pushing the catheter shaft, the unsupported portion of the catheter shaft tends to buckle within the guide catheter. Buckling of the catheter shaft within the guide catheter increases the number and area of points of contact between the catheter shaft and the inner surface of the guide catheter lumen, thus increasing friction and causing the balloon catheter to bind up in the guide catheter and impairing the ability of the catheter to be pushed along the guidewire. The tendency to become bound up in the guide catheter increases with the extent to which the catheter is advanced through the guide catheter and prevents the catheter from being advanced into distal coronary vasculature.

The tendency for the dilatation catheter shaft to buckle is particularly acute in the region of the aortic arch.

It is among the general objects of the invention to provide an improved PTCA catheter having a rapid exchange feature which avoids the foregoing and other difficulties.

It is among the general objects of the invention to provide an improved rapidly exchangeable balloon dilatation catheter.

Another object of the invention is to provide a rapidly exchangeable balloon dilatation catheter which is provided with axial support along the full length of the catheter.

Another object of the invention is to provide a rapidly exchangeable balloon dilatation catheter which is provided with axial support along the full length of the catheter.

Another object of the invention is to provide a rapidly exchangeable catheter having a relatively flexible distal portion that receives a guidewire and is of sufficient length that it can extend from the distal coronary anatomy over the aortic arch and into the descending aorta.

A further object of the invention is to provide a rapidly exchangeable catheter having an elongate moderately flexible self-supporting proximal section and at least one distal section that is more flexible and has a guidewire lumen extending therethrough whereby the guidewire may support said distal segments.

A further object of the invention is to provide a rapidly exchangeable catheter which has a reduced tendency to buckle within the guide catheter.

Another object of the invention is to provide a rapidly exchangeable catheter which provides reduced friction in the guide catheter.

A further object of the invention is to provide a rapidly exchangeable catheter which better enables the physician to advance the distal end of the catheter into the distal coronary anatomy of a patient.

According to one aspect of the invention, there is provided a catheter for accessing the coronary arteries in a human comprising an elongate proximal segment including a relatively stiff tube, a relatively flexible elongate plastic distal tubular member mounted to the distal end of the proximal segment, the plastic member being more flexible than the proximal segment and having a guidewire lumen formed therethrough, the guidewire lumen having a proximal opening in the region of the juncture of the plastic member and the proximal segment and having a distal opening at its distal end whereby when a guidewire is contained within the lumen, the catheter will have continuous longitudinal support from its proximal end to its distal tip and means carried by the distal end of the

plastic distal tubular member for performing a procedure in a coronary artery.

Preferably, the means for performing a procedure in an artery comprises a dilatation balloon and where the proximal segment and the plastic distal tubular member have an inflation lumen communicating the interior of the balloon with the proximal end of the catheter.

Conveniently, the plastic segment is approximately 40cm long.

According to another aspect of the invention there is provided a rapidly exchangeable balloon dilatation catheter for accessing the coronary arteries of a human comprising an elongate wire-like shaft having proximal and distal ends and including a proximal tubular member formed from hypotubing, the shaft having sufficient column strength to enable it to be advanced through a patient's vasculature to the coronary arteries, the proximal tubular member having a lumen extending therethrough, a distal tubular member secured to the distal region of the shaft and sufficiently flexible to access the coronary arteries but itself having insufficient column strength for such access without additional support, the distal tubular member having an inflation lumen extending longitudinally therein and having a proximal end in fluid communication with the lumen of the hypotubing, the inflation lumen being in communication with a balloon inflation port, the distal tubular member including a longitudinally extending guidewire lumen receptive to a guidewire and having a distal port and a proximal port, the guidewire lumen extending from the distal region of the shaft to the distal end of the catheter and over a distance sufficient, when a guidewire is positioned through the guidewire lumen, to increase the column strength of the distal tubular member, the guidewire and the shaft together supplying support along the length of the catheter, and an inflatable, relatively inelastic balloon mounted on the distal tubular member, having a distal end sealingly attached to the distal end of the distal tubular member and an interior in fluid communication with the inflation lumen through the inflation port.

Preferably, the elongate wire-like shaft is of a smaller diameter than the distal tubular member.

Suitably, the catheter includes a guidewire extending through the guidewire lumen.

Preferred embodiments of the invention will now be described, by way of example only, with reference to the accompanying drawings wherein:

FIG.1 is a fragmented illustration of the catheter; FIG.2 is an enlarged illustration of the catheter; FIG.3 is a diagrammatic illustration of a patient showing the manner in which a balloon catheter is advanced from the femoral artery through the aorta to the patient's heart;

FIG.4 is an illustration of the aorta leading from the heart and coronary arteries with a guide catheter in place and the catheter of the present invention extending through the guide catheter; FIG.5 is a cross-sectional illustration of the two lumen segment of the intermediate segment of the catheter as seen along the line 5-5 of FIG.2; FIG.6 is an enlarged illustration of the proximal end of the balloon and its point of attachment to the intermediate segment; FIG.7 is a sectional longitudinal illustration of the catheter in the region where the proximal metal tubular segment is joined to the intermediate more flexible plastic segment; and FIG.8 is an enlarged longitudinal sectional illustration of the distal end of the catheter showing the balloon and the manner of its attachment to the intermediate and distal segments.

Figure 3 illustrates, diagrammatically, a conventional over-the-wire balloon dilatation catheter 10 and a guidewire 12 inserted onto the patient's vasculature through a guide catheter 14. The guide catheter 14 is initially placed, percutaneously, into the patient's femoral artery 16 and is advanced along the descending aorta 18 over the aortic arch 20 and into the ascending aorta 22 that leads from the heart 24. As will be appreciated by those skilled in the art, the distal end of the guide catheter is specially shaped so that the distal tip 23 of the guide catheter will easily lodge in the entrance to the right 25 or left 27 coronary artery (see Figure 4).

When it is desired to exchange the balloon catheter 10 for another, it is important that the guidewire 12 be maintained within the patient's artery so that it may guide the next succeeding catheter quickly and efficiently to the intended site in the patient's vascular system. Typically, the clearances between the guidewire 12 and the inner lumen of the catheter 10, coupled with the bends which the catheter 10 and guidewire 12 must follow along the patient's artery are such that withdrawal of the catheter 10 tends to drag the guidewire 12 out with the catheter 10. In order to maintain the guidewire 12 in place while the catheter 10 is withdrawn, it is necessary to hold the guidewire 12 by its proximal end while withdrawing the catheter 10 over the guidewire 12.

Among the techniques for facilitating a catheter exchange is the use of a monorail-type of catheter in which the guidewire lumen in the catheter extends only over a relatively short length of the catheter at the distal end of the catheter. Because the guidewire lumen is shorter than the portion of the guidewire that protrudes out of the patient, some part of the guidewire is always exposed and may be grasped to maintain guidewire position. With the monorail system, it is unnecessary to use

exchange wires or other devices to increase the effective length of the guidewire in order to perform a catheter exchange.

Figure 2 is a fragmented illustration of a catheter in accordance with the invention. The catheter 26 includes an elongate proximal segment 28 which is formed from metallic hypodermic tubing, preferably stainless steel. The proximal segment may be of the order of 100 to 110 cm long. The tubing 28 may be of the order of 0.56mm (0.022") outer diameter with a wall thickness of about 0.076mm (0.003"). The catheter 26 also includes an intermediate segment 30 attached at its proximal end to the distal end of the metal tube 28 and being shorter in length than the metal tube 28. The catheter also includes a distal segment 32 (Figures 2 and 8) attached to the distal end of the intermediate segment 30. A dilatation balloon 34 is mounted on the distal segment 32 as will be described. The metallic tubular proximal segment 28 defines a lumen 36 (Figure 7) that extends fully through its length. A luer fitting 38 is attached to the proximal end of the tubing 28 to connect the lumen 36 with an inflation/deflation device, such as a syringe (not shown). The lumen 36 communicates with a lumen 40 in the intermediate segment 30. The lumen 40 terminates at a port 42 disposed within the balloon 34. Thus, the balloon 34 may be inflated and deflated through the inflation/deflation lumens 36,40 in the metal tube 28 and intermediate segment 30, respectively.

As will be described, the metal tubular segment 28 provides for a high degree of column strength and enables the catheter to be pushed from its proximal end without buckling. The metal tube 28 may be coated with a thin film of lubricious material, such as Teflon, polytetrafluoroethylene.

The flexible plastic intermediate segment 30 may be an extruded tube of suitable plastic such as high density polyethylene. The intermediate segment 30 may be of the order of 1.14mm (.045") outer diameter. The length of the intermediate segment 30 is between about 30 to 40cm for reasons discussed below. The intermediate segment 30 has two lumens including the inflation lumen 40 which may be somewhat D-shaped as illustrated in Figure 5. The other lumen 44 may be circular as shown in Figure 5 and is adapted to receive the guidewire 12. The guidewire lumen 44 may be of the order of 0.51mm (.020") diameter. The guidewire lumen terminates in a proximal opening 46 so that the guidewire is exposed proximally of the intermediate segment 30. Thus, the guidewire may extend within the guide catheter 14 in parallel to and outside of the proximal segment 28.

The distal segment 32 of the catheter is formed from a separate length of single lumen tubing which may be extruded from a relatively

flexible plastic material such as low density polyethylene. The distal segment 32 is circular in cross-section and has a circular lumen 48 Figure 6 which is an extension of the guidewire lumen 44 in the intermediate segment 30. The distal tip of the distal segment 32 is open at a distal outlet orifice 33 Figure 8. The distal segment 32 may be attached by fusing its proximal end to the distal end of the intermediate segment 30 while maintaining continuation of the guidewire lumen 44,48 and the opening 42 of the inflation lumen 40 by inserting mandrels in those lumens during the fusion process. A highly radiopaque marker band preferably is mounted on the distal segment 32 and is encapsulated in an overlying thin polyethylene sleeve 37, the sleeve 37 extending proximally over the joint 39 between the intermediate segment 30 and distal segment 32. The sleeve 37 also is heat fused to the shaft. The distal segment 32 may have a wall thickness of the order of 0.089mm (.0035") thereby making it more flexible than the more massive intermediate segment 30. A radiopaque marker band 35 formed from an appropriate radiopaque material, such as gold or platinum, may be mounted on the distal segment 32.

The balloon 34 is mounted on the distal region of the catheter. The balloon 34 may be formed from a suitably flexible strong and relatively inelastic material such as polyethylene terephthalate. The balloon may be formed in a procedure described in US-A-4,490,421 to Levy. The balloon may be of the order of 20mm long and may have a balloon diameter when inflated of from about 1.5mm to 4.0mm. The wall thickness may be of the order of 0.013-0.026mm (0.0005" to 0.001"). The balloon includes an elongate cylindrical portion having integral tapering conical sections 49,51 at each of its proximal and distal ends. Each of the conical sections merges into a small diameter cylindrical neck, the neck 52 at the proximal end of the balloon being larger in diameter than the neck 54 at the distal end. The proximal neck 52 is mounted on the distal region of the intermediate segment 30 and the distal neck 54 is mounted on the distal portion of the distal segment 32. The neck portions 52,54 are securely bonded to the intermediate and distal segments 30,32, respectively, by an appropriate adhesive such as an epoxy.

The manner in which the catheter of the present invention is used will be appreciated from Figures 3 and 4. In a typical procedure, the femoral artery 16 is accessed percutaneously by a hollow needle. After inserting the needle into the femoral artery, a relatively large diameter guidewire 0.97mm (about 0.038" diameter) is advanced through the needle and into the femoral artery. The needle is removed and an introducer sheath and dilator are placed inside the artery. The dilator is

then removed. The guide catheter is inserted over the guidewire and is advanced along with the guidewire to the ascending aorta when the 0.97mm (.038") guidewire is removed. The distal end of the guide catheter 14 is shaped specially to be easily inserted into the entrance of one of the two coronary ostia to access either the right or left main coronary arteries. Figure 4 illustrates a guide catheter 14 seated in the left coronary ostium. Once the guide catheter is in place, the 0.97mm (0.038") guidewire may be removed. The guide catheter 14 then is ready to receive the dilatation catheter and its small diameter e.g. 0.25-0.46mm (.010"-018") diameter guidewire.

In placing the small diameter steerable guidewire 12 and the conventional over-the-wire balloon dilatation catheter 10, it is conventional practice to first assemble the guidewire 12 with the balloon catheter 10 and then pass them both in unison through the guide catheter. Alternately, with the present invention, the guidewire 12 may be inserted through the guide catheter by itself. The guidewire is advanced to the coronary ostium and then may be further advanced into the coronary arteries. The guidewire may be of the type described in US-A-4,545,390 to Leary and may be steerable so that it can be manipulated and guided to the desired branch of the coronary arteries to be treated. The progress of the guidewire through the patient's coronary arteries may be monitored fluoroscopically by the physician. The physician also may inject radiopaque contrast liquid through the guide catheter to visualize the coronary anatomy on the fluoroscope. Once the guidewire 12 has been advanced through the stenosis to be treated, the balloon catheter 26 of the present invention is advanced over the guidewire 12 and within the guide catheter 14. The catheter 26 will track smoothly and easily along the guidewire with no significant tendency to buckle. This results from the relatively stiff, pushable nature of the elongate metal tubular proximal segment 28 of the catheter. Additionally, the intermediate and distal segments 30,32 are supported by the guidewire 12 which provides significant resistance to buckling of the intermediate and distal segments 30,32. It will be appreciated, therefore, that when the catheter 26 is advanced over the guidewire, the catheter will have significant axial, column support fully along its length. In this regard, it is important to note that the proximal end of the guidewire lumen 44 in the intermediate segment 30 overlaps longitudinally, the distal end of the metal tubular proximal segment 28 that is embedded in the proximal end of the intermediate segment 30. Thus, when the catheter is advanced over the guidewire 12, there is column support fully along the length of the catheter, from its proximal to its distal end. As a result,

there is considerably reduced tendency for any portion of the catheter to buckle longitudinally. Consequently, the friction between the balloon dilatation catheter 26 and the guide catheter 14 is substantially reduced thereby enabling the distal end of the catheter to be advanced into distal, remote and tortuous regions of the patient's coronary anatomy.

In order to better grasp the proximal end of the catheter to push it through the guide catheter, a gripping device 56 may be mounted on the proximal segment 28. The gripping device 56 includes a nut 58 which is threaded into a tubular collet 60. The collet 60 and nut 58 are screwed together over the proximal segment 28 to cause the collet 60 to securely grip the proximal segment 28. The position of the gripping device 56 may be adjusted by loosening the nut and repositioning the device.

It should be noted that the length of the intermediate and distal segments 30,32 are selected so that when the balloon is placed in a very distal region of the coronary anatomy, the juncture of the proximal end of the intermediate segment with the proximal tubular segment 28 is disposed in the descending aorta 18 and does not extend into the aortic arch 20. Thus, the combined length of the intermediate and distal segments 30,32 should be between 35 to 45 cm long, with a length of 40 cm being preferred for most patient's anatomies. It will be appreciated from the foregoing construction that the flexible intermediate and distal portions 30,32 will pass easily through the curve of the aortic arch 20 without tendency to buckle because they are fully supported by the guidewire 12. The relatively stiff elongate metal proximal segment 28 does not pass through the aortic arch 20 and maintains its relatively straight configuration so that its pushable characteristics are not compromised. There is minimal tendency of the catheter to dislodge the distal tip of the guide catheter from its position in the coronary ostium.

Should it be desired to exchange the balloon catheter 26 for another catheter, there is no need to use an extended length guidewire. Typically, about 50 cm of the guidewire 12 will protrude exteriorly of the patient. When the catheter 26 is withdrawn, a segment of the guidewire 12 will be exposed at all times, thereby enabling the guidewire 12 to be grasped to maintain its position in the patient. Thus, the catheter 26 may be withdrawn without dragging the guidewire 12 out of position. After the first catheter has been removed, another catheter may be threaded onto the guidewire and advanced through the guide catheter and into the coronary anatomy, guided by the guidewire 12. The catheter constructed in accordance with the invention will be advanced easily, without tendency to buckle or develop high friction

within the guide catheter and with no significant tendency to dislodge the guide catheter from its position at the coronary ostium.

From the foregoing, it will be appreciated that the invention provides an improved rapidly exchangeable catheter construction and catheterization method.

It should be understood, however, that the foregoing description of the invention is intended merely to be illustrative thereof.

For example, although the invention has been illustrated in connection with a balloon dilatation catheter, it may also be incorporated in other types of catheters, such as laser catheters, hot tip catheters, infusion catheters, arterectomy catheters and the like.

Claims

1. A rapidly exchangeable balloon dilatation catheter for accessing the coronary arteries of a human comprising:
 - an elongate wire-like shaft having proximal and distal ends and including a proximal tubular member formed from hypotubing (28), the shaft having sufficient column strength to enable it to be advanced through a patient's vasculature to the coronary arteries, the proximal tubular member having a lumen (36) extending therethrough;
 - a distal tubular member (32) secured to the distal region of the shaft and sufficiently flexible to access the coronary arteries but itself having insufficient column strength for such access without additional support, the distal tubular member (32) having an inflation lumen (40) extending longitudinally therein and having a proximal end in fluid communication with the lumen (36) of the hypotubing, the inflation lumen (40) being in communication with a balloon inflation port (42);
 - the distal tubular member (32) including a longitudinally extending guidewire lumen (44) receptive to a guidewire (12) and having a distal port (33) and a proximal port (46), the guidewire lumen (44) extending from the distal region of the shaft to the distal end of the catheter and over a distance sufficient, when a guidewire (12) is positioned through the guidewire lumen, to increase the column strength of the distal tubular member (32), the guidewire and the shaft together supplying support along the length of the catheter; and
 - an inflatable, relatively inelastic balloon (34) mounted on the distal tubular member (32) having a distal end (54) sealingly attached to the distal end of the distal tubular member (32) and an interior in fluid communication with the

inflation lumen (40) through the inflation port (42).

2. A balloon dilatation catheter as claimed in claim 1 characterised in that the elongate wire-like shaft is of smaller diameter than the distal tubular member (32). 5
3. A catheter for accessing the coronary arteries in a human comprising: 10
 - an elongate proximal segment including a relatively stiff tube (28);
 - a relatively flexible elongate plastic distal tubular member (32) mounted to the distal end of the proximal segment, the plastic member being more flexible than the proximal segment and having a guidewire lumen (44) formed therethrough, the guidewire lumen having a proximal opening (46) in the region of the juncture of the plastic member and the proximal segment and having a distal opening (33) at its distal end whereby when a guidewire is contained within the lumen, the catheter will have continuous longitudinal support from its proximal end to its distal tip; and 15
 - means carried by the distal end of the plastic distal tubular member (32) for performing a procedure in a coronary artery. 20
4. A catheter as defined in claim 3 characterised in that the means for performing a procedure in an artery comprises a dilatation balloon (34) and where the proximal segment and the plastic distal tubular member (32) have an inflation lumen communicating the interior of the balloon with the proximal end of the catheter. 25
5. A catheter as defined in claim 3 or claim 4 characterised in that the plastic segment is between 35 to 45 cm long. 30
6. A catheter as claimed in any preceding claim characterised by a guidewire (12) extending through the guidewire lumen. 35

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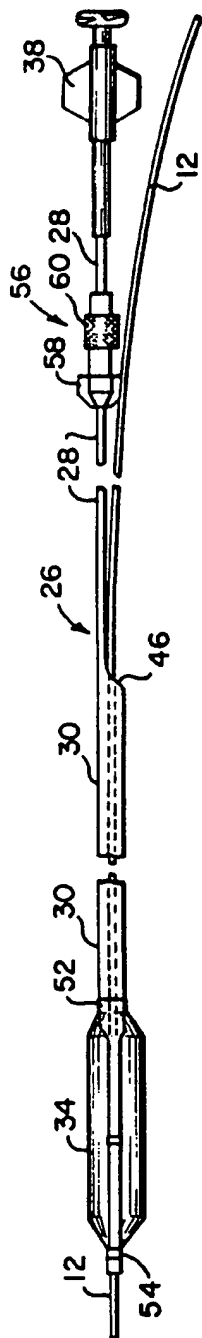


Fig. 1

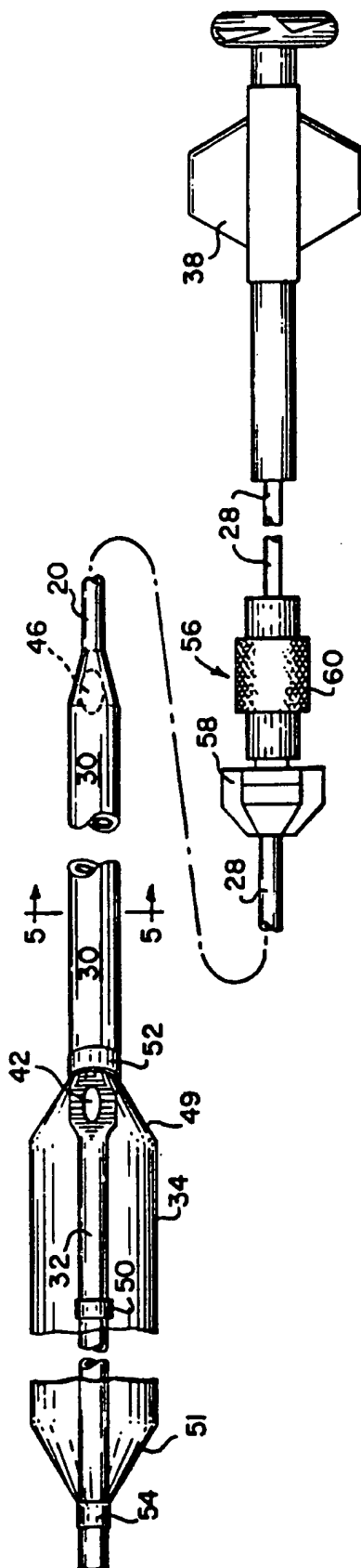
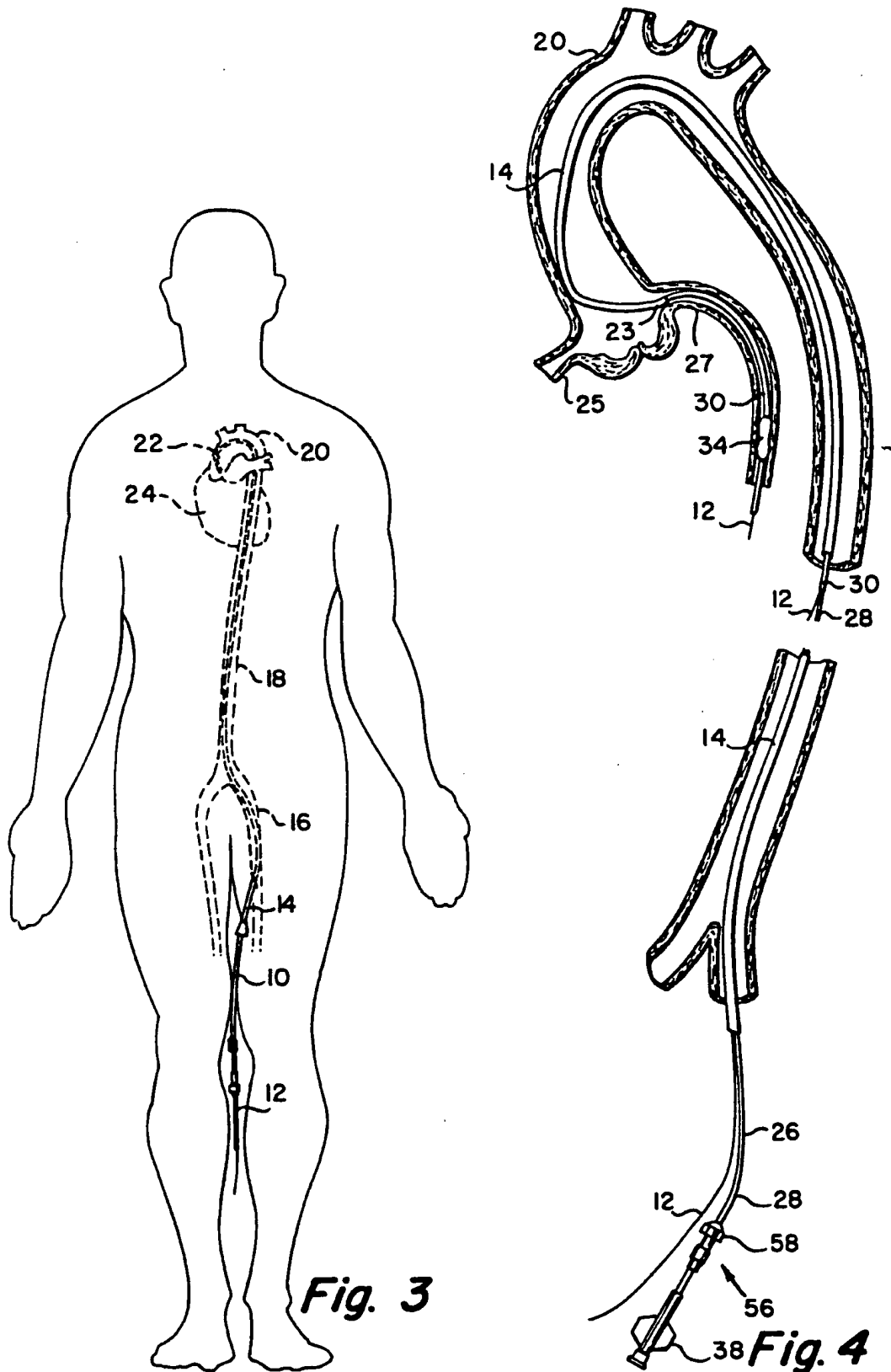


Fig. 2



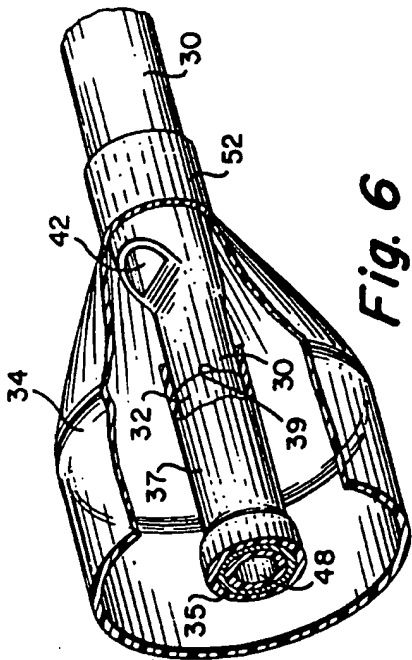


Fig. 6

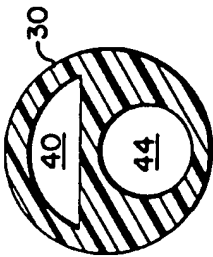


Fig. 5

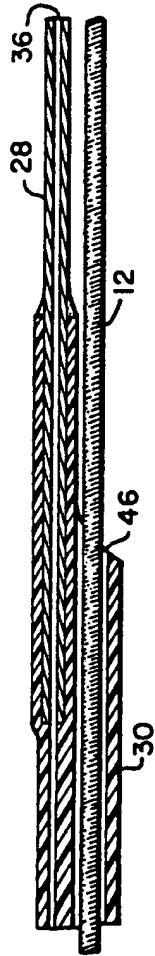


Fig. 7

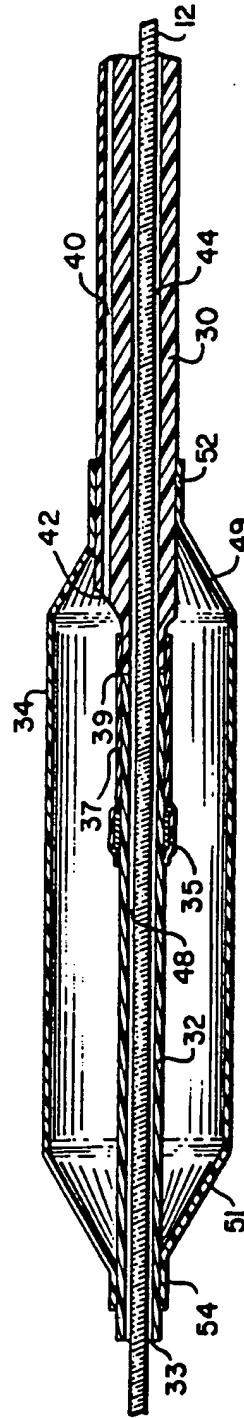


Fig. 8



European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 93 11 9677

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.5)
X	EP-A-0 274 129 (ADVANCED CARDIOVASCULAR SYSTEMS, INC.) * the whole document * ---	1,3-6	A61M29/02
A	US-A-4 652 258 (DRACH) * column 2, line 56 - column 3, line 34; figures 6,7 * -----	1-6	
			TECHNICAL FIELDS SEARCHED (Int.Cl.5)
			A61M
The present search report has been drawn up for all claims			
Place of search THE HAGUE		Date of completion of the search 17 February 1994	Examiner Mir y Guillen, V
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons @ : member of the same patent family, corresponding document			